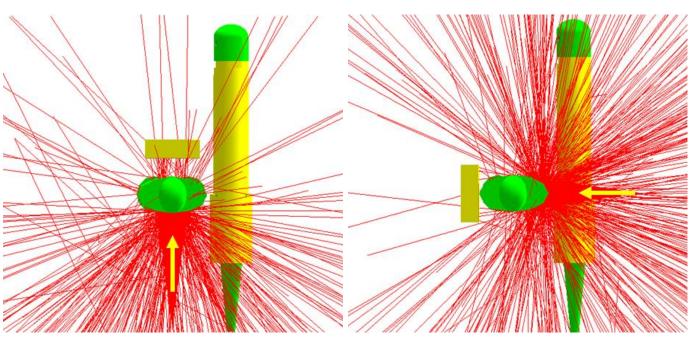
# Staff shielding of the eye lens and brain

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With the collaboration of C. J. Martin, F. Vanhavere, J. Dabin and N. Buls

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#### Introduction



Monte Carlo simulation of an interventional cardiology procedure. Red lines are particle tracks

- Staff: radiation scattered by the patient
- Heterogeneous radiation field
- Head: mostly unshielded

- Eye lens: high radiosensitivity => cataracts
- Brain: still controversial; solid cancer risk?
  vascular risk?

#### Introduction

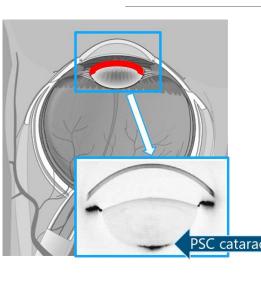


Table 1. Mean measured  $H_p(3)$  per procedure  $\pm 1$  s.d., number of procedures per year and estimated annual dose for Radiation Protection Dosimetry (2015), physicians.

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	$< H_p(3)/\text{proc}> \pm 1 \text{ s.d.}$ in $\mu \text{Sv}$	No. proc	$H_{\rm p}(3)  {\rm y}^{-1}  {\rm in}$ mSv
Phys. 1	164 ± 129	369	61 🛨
Phys. 2	$42 \pm 39$	303	13
Phys. 3	$218 \pm 163$	149	32
Phys. 4	$62 \pm 45$	253	16
Phys. 5	$45 \pm 42$	182	8
Phys. 6	$49 \pm 46$	253	12
Phys. 7	$65 \pm 53$	325	21 🛨
Phys. 8	$251 \pm 187$	77	19 ←
Phys. 9	$130 \pm 102$	385	50 ←

Dose limit: 20 mSv/year

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- Brain: still controversial; solid cancer risk?
  vascular risk?

#### Is brain cancer an occupational disease of cardiologists?

Finkelstein MM<sup>1™</sup>

The Canadian Journal of Cardiology, 01 Nov 1998, 14(11):1385-1388 PMID: 9854520

#### Objective

To assess the plausibility of radiation as a cause of the statistically unusual event of two cardiologists in Toronto, Ontario who were diagnosed with brain tumours in 1997.

#### Conclusions

Initiation of brain tumours during cardiac fluoroscopic procedures is plausible. Physicians are reminded to practise radiation safety methods during fluoroscopic procedures. The diagnosis of two additional brain tumours in Canadian interventional cardiologists during the past 10 years would confirm the occupational causation theory. The author invites physicians to report knowledge of the diagnosis of brain tumours in Canadian cardiologists to the author or to the editors.

Data suggest that the vasculature in the brain may show damage at doses as low as 150 mSv (or 150,000 µSv).

JACC: CARDIOVASCULAR INTERVENTIONS VOL. 9, NO. 3, 2016 FEBRUARY 8, 2016:299-304 Letters to the Editor

#### Introduction

Radiation Protection of the head: eye lens and brain

- Lead glasses
- Masks
- (Caps)









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- Different models of lead glasses available
- Models from before the ICRP dose reduction
- Efficiency assessed with phantoms, dosemeters over the eye surface
- Dose Reduction Factor: ~ 1 10



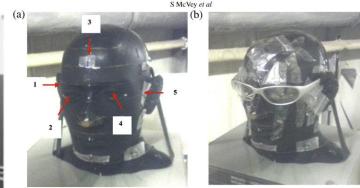
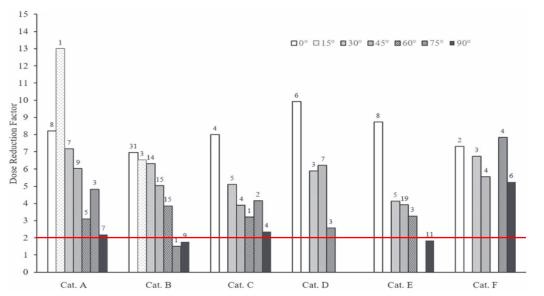


Figure 2. (a) Rando head phantom showing TLD positions 1–5.1: RHS, 2: Right eye, 3: forehead, 4: left eye, 5: LHS, (b) Rando head phantom measurements with protective lead glasses.

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**Figure 2.** Mean of the *DRF* estimates aggregated by horizontal scatter incidence angle  $\alpha_h$  and eyewear category. The numbers on the top of the columns represent the sample size for each group.

Radiation direction	Dose transmission factor (%) for eight models of eyewear									
	1	2	3		4	5	5	6	7	8
Below, left lens	72	43	78		85	8	36	22	35	70



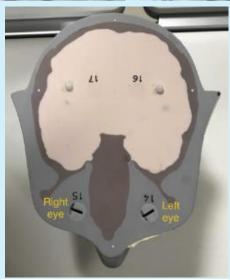
Figure 4. Head phantom



Figure 6. Polyethylene disc, used in the head phantom, with holes to fit TLDs.

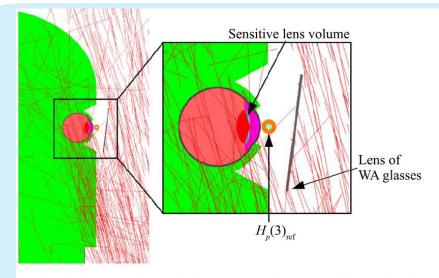
Eyewear	Left lens		
Standard eyewear	99% ± 4%		
Eyewear with side shield	96% ± 5%		





J Vasc Surg. 2020 Dec;72(6):2139-2144.

T. Geber et al. / Radiation Measurements 46 (2011) 1248-1251

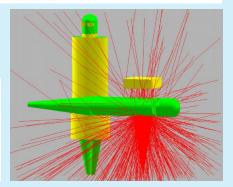


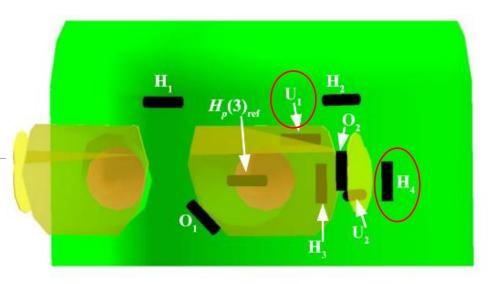
**Figure 4.** Shielding provided by the lead glasses to  $H_p(3)_{ref}$  and to the eye lens. Lines represent x-ray photon tracks, simulated with MCNPX.

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$$\frac{H_p(3)_{ref}}{H_{lens,sensitive}} = 0.6$$







**Figure 3.** Positions of dosemeters modelled in the simulations. The dosemeters are shown as black where viewed directly and the colour modified where they are overlaid by shields.

Position	$R_{H_{\mathrm{lens}}}$
$H_1$	1.3
$H_2$	1.0
$H_3$	1.6
$H_4$	1.5
$O_1$	1.6
$O_2$	1.5
$U_1$	0.2
$U_2$	0.4
$H_p(3)_{\text{ref}}$	0.6

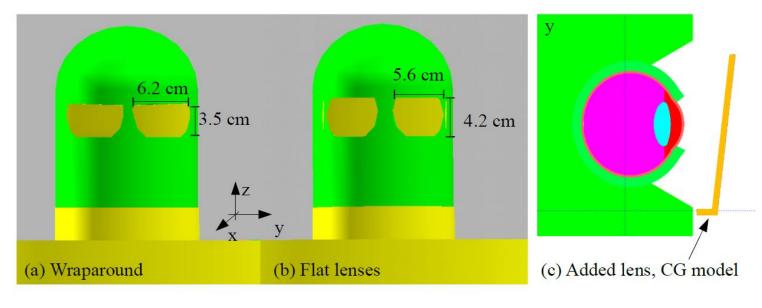
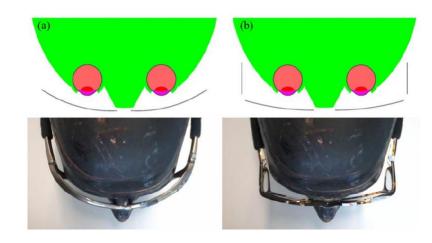
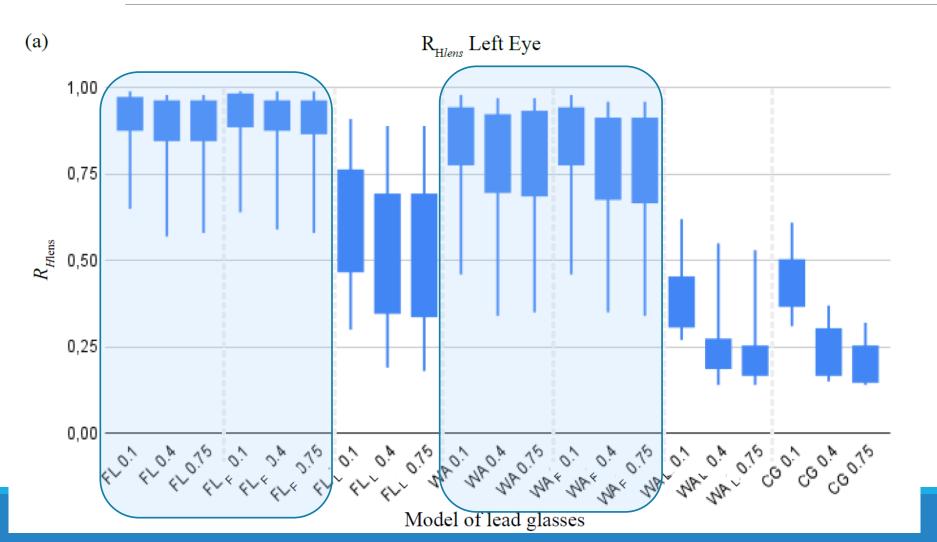
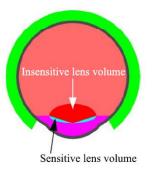


Figure 1: Dimensions of the two standard models of lead glasses: a) Wraparound (WA) and b) flat frontal lenses with side shielding (FL). c) Added lead rims towards the face in the CG model, transverse view.

- Variation in the design of lead glasses
  - Lead thickness
  - Presence of Pb in the frames
  - Lens length
  - Extra horizontal lens







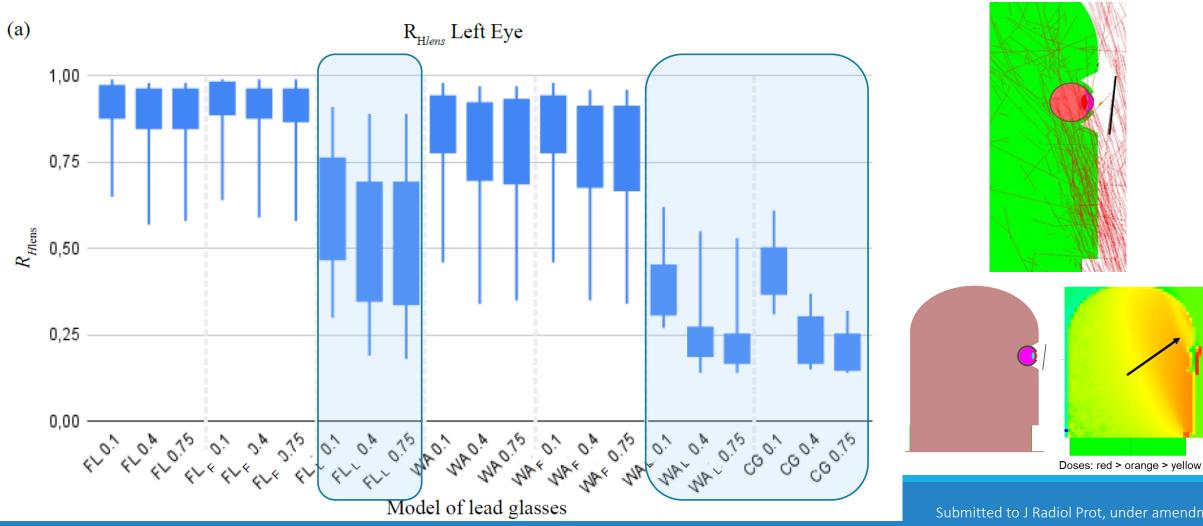
Average  $R_{Hlens}$ : 0,77 – 0,92

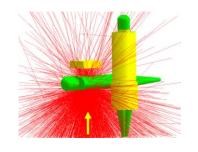
Lens thickness: 0,1 mmPb to 0,75 mmPb

Presence or absence of Pb In the frames

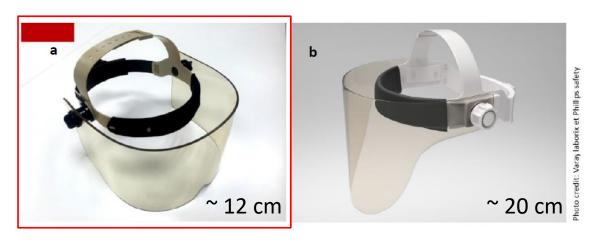
Average  $R_{Hlens}$ : 0,20 – 0,62

Longer frontal lens: 1 to 2 cm, depending on the model of LG





### Eye lens and brain protection

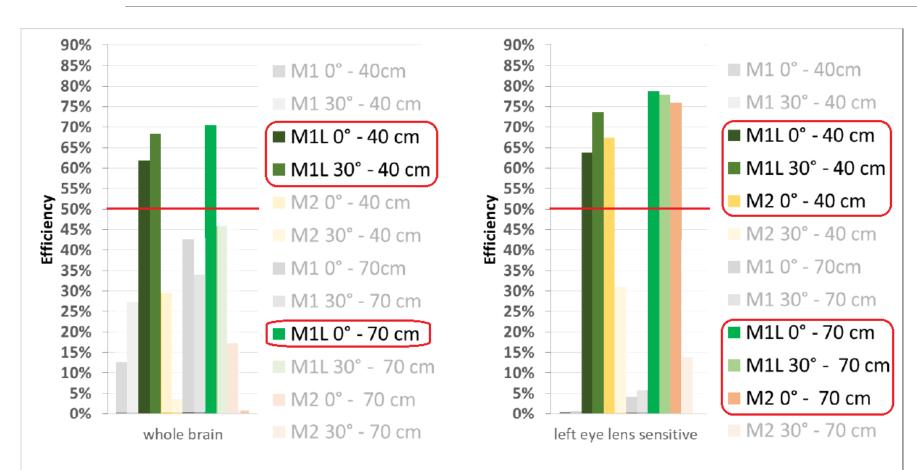


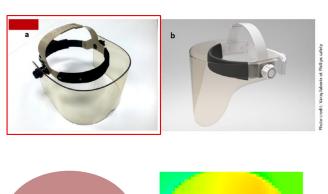
Attenuation (dosemeters on the mask) M1 (a) = 76% to 87% M2 (b) = 65% to 90%

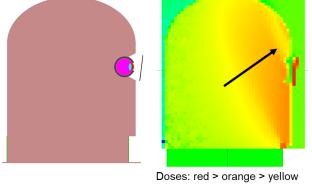
M1 efficiency for brain, eye lens for PA projection and four operator positions (head at 0°)

	Whole brain	Left eye lens
PA -40 cm	11.6%	0.1%
PA-50 cm	20.3%	1.2%
PA – 60 cm	31.6%	1.8%
PA – 70 cm	39.2%	1.9%

## Eye lens and brain protection







#### Summary

#### Lead glasses:

- current models decrease the eye lens dose by only 20%
- Models with longer frontal lens, even of thinner Pb equivalency, are potentially more efficient (dose reduction > 50%)

#### Masks:

- Longer models provide better protection for eye lens and brain (dose reduction > 50%)
- Attenuation measured with dosemeters over/under the mask is not realistic of their efficiency (+65% vs 5% to 40%)

#### Caps:

- Provide some protection only to the brain, none to the eye lens
- Attenuation measured with dosemeters over/under the cap is not realistic of their efficiency (~80% vs < 40%)</li>

Efficiency of RP devices *usually* increases further from the primary X-ray beam (femoral access)

# Take Home message

- Attenuation is NOT the same as dose reduction in the organ of interest
- Dose reduction assessment is STRONGLY influenced by the reference dose
- Radiation reaching the staff comes from below: minimizing spaces where radiation can leak through will likely increase protection

There is still room for optimization of radiation protection devices!

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